

# Mechanical feedback as a possible regulator of tissue growth

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**Regulation of cell growth and proliferation has a fundamental role in animal and plant development and in the progression of cancer. In the context of development, it is important to understand the mechanisms that coordinate growth and patterning of tissues. Imaginal discs, which are larval precursors of fly limbs and organs, have provided much of what we currently know about these processes. Here, we consider the mechanism that is responsible for the observed uniformity of growth in wing imaginal discs, which persists in the presence of gradients in growth inducing morphogens in spite of the stochastic nature of cell division. The phenomenon of “cell competition,” which manifests in apoptosis of slower-growing cells in the vicinity of faster growing tissue, suggests that uniform growth is not a default state but a result of active regulation. How can a patch of tissue compare its growth rate with that of its surroundings? A possible way is furnished by mechanical interactions. To demonstrate this mechanism, we formulate a mathematical model of nonuniform growth in a layer of tissue and examine its mechanical implications. We show that a clone growing faster or slower than the surrounding tissue is subject to mechanical stress, and we propose that dependence of the rate of cell division on local stress could provide an “integral-feedback” mechanism stabilizing uniform growth. The proposed mechanism of growth control is not specific to imaginal disc growth and could be of general relevance. Several experimental tests of the proposed mechanism are suggested.**

*Drosophila melanogaster* | imaginal disc | mechanics | stress

Understanding the principles and mechanisms involved in animal and plant development remains an outstanding challenge for modern biology (1, 2). Among the fundamental problems is the problem of understanding how organisms (or organs and body parts) coordinate their growth with internal patterning to achieve correct size and proportions (3–5). A fruit fly, *Drosophila melanogaster*, has been an invaluable model of development in general and organogenesis in particular (6, 7). Below, we focus on the question of growth control (8, 9) in the context of a wing imaginal disc (7), which is the larval precursor of the adult wing. We point out that nonuniform growth in a layer of cells that adhere to each other (as is the case for imaginal discs) leads to accumulation of mechanical stress. This stress may provide cells with a feedback signal, regulating cell division and insuring stable and uniform growth of tissue. To describe this process quantitatively, we formulate and analyze a mathematical model of mechanical deformation in growing tissue. We show that the proposed mechanical feedback model could naturally explain certain salient features of growth in imaginal discs, such as “cell competition” (6, 10, 11), and suggest experiments that would directly test the model.

The possible role of mechanical interactions in growth has been suggested, most explicitly in the context of plant development (12–15). However, mechanics has been demonstrated to have a role in regulation of cellular processes in animals as well. Specialized mechanosensory cells use mechanically gated ion channels as sensors (16, 17). Compressive and tensile stresses are known to be important in muscle and bone tissues and tension-sensitive signaling has been reported in tissue cultures (18–20).

Also suggestive of mechanical interactions are the observations of the effects of geometric constraints on the growth of cultured endothelial cells (21). Focal adhesion complexes and adherens junctions (through which cells interact with the substrate and each other, respectively) have been argued as the likely loci of mechanosensation (22, 23). There is evidence for mechanical stress-induced ectopic expression of genes in *Drosophila* embryo (24), which appears to be mediated by Armadillo, a protein that in one of its roles serves as a scaffold for the assembly of cell-adhesion junctions with cortical actin (25, 26). And most recently, a link between mechanical deformation, actin cytoskeleton morphology, and transcription factors [Mal-D and serum response factor (SRF)] has been demonstrated in the migrating border cells during *Drosophila* oogenesis (27). On the theory side, modeling of tissue mechanics during development has been discussed before in the context of convergent extension (28) and in the context of cell sorting and differential adhesion (29–31).

Wing imaginal disc derives from a patch of  $\approx 50$  embryonic cells, which by the time of growth arrest occurring at pupation, will multiply by means of cell division to  $\approx 5 \times 10^4$  (7). Patterning of imaginal discs proceeds concurrently with growth, although at that stage it is evident only on the level of gene expression. The pattern of expression of certain key transcription factors is organized relative to antero-posterior and dorso-ventral axes (32–34) and is generated in response to gradients in concentration of morphogens (35): Decapentaplegic (Dpp) (32, 33) for antero-posterior and Wingless (34, 36) for the dorso-ventral axes. Notably, both morphogens are also required for tissue growth (37, 38).

A very appealing proposal for a mechanism of size determination exists (3, 35, 39); the idea is that growth is controlled by a gradient of “positional values.” Positional value is a yet unidentified property of the cell, which becomes a fixed attribute of the cell upon the birth of the cell, with its value interpolating those of neighboring cells (3, 35, 39). As tissue grows, new cells intercalate between cells, gradually decreasing positional value differential between neighboring cells until it falls below a threshold and growth stops (39). The most explicit scenario of this type (3) suggests that the role of positional value is played by the morphogen concentration itself and, hence, that growth is driven by morphogen gradient. This idea is appealing because it offers an explicit link between growth and patterning of gene expression. However, this scenario is contradicted<sup>‡</sup> by experimental observation that Dpp, and not its gradient, drives cell proliferation (32, 40).

The observation that growth is driven directly by morphogen level leads to another puzzle. The rate of proliferation within the wing pouch of the imaginal disc is observed to be on average

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Abbreviation: Dpp, Decapentaplegic.

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<sup>‡</sup>Another problem involves the proposed notion that morphogen gradient decreases in inverse proportion with the size of the tissue. The latter behavior does not follow from the laws of diffusion without an additional assumption that the rate of Dpp secretion at the antero-posterior boundary itself decreases in inverse proportion with the size.

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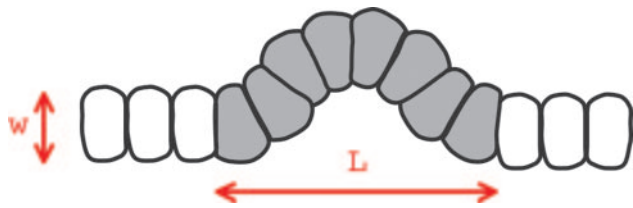


Fig. 2. Schematic representation of a cross-section of a buckled region of a cell layer.

avoid excessive local compression and buckling. Actually, tissue growth regulation may be broken down into three distinct components, (i) regulation of cell division rate, (ii) regulation of cell growth rate, and (iii) activation of apoptosis. The  $\gamma(r, t)$  variable represents their combined effect (as explained in *Supporting Appendix*).

### Mechanical Feedback Mechanism

Any mechanism coordinating growth within tissue would require an input signal containing information that allows each cell to compare its rate of growth and division with that of the surrounding tissue. Mechanical interactions are very interesting in this respect, because they immediately provide information that is necessary for a regulatory feedback mechanism.<sup>||</sup> For example, suppose that local tissue growth rate  $\gamma(r, t, p(r, t))$  depends explicitly on the degree of local compression (or stretching) of the tissue as quantified by  $p(r, t)$  and this dependence has a form as shown in Fig. 3, which assumes only that (i) growth rate depends on pressure and (ii) large mechanical stress suppresses growth and triggers apoptosis (which corresponds to  $\gamma < 0$ ). Given the dependence of pressure on the growth-rate differential described by Eq. 1, we show in Fig. 3 how mechanical feedback could robustly lead either to the equilibration of growth rates or elimination of growth-impaired clones.

According to the feedback scenario shown in Fig. 3, a faster-growing clone would be larger than the WT clone of the same “age,” but the difference would not be increasing exponentially in time, as might be expected on the basis of different growth rates. Instead, the mutant clone would be larger than WT by a fixed factor (see Fig. 4a), the magnitude of which depends on the strength of the feedback (i.e., sensitivity of growth rate to pressure given by the blue curve in Fig. 3) and shear rigidity of tissue,  $\mu$ . For a slow-growing clone, the analysis shown in Fig. 3 predicts inevitable death by apoptosis.

The regulatory feedback mechanism proposed above involves the integral of the difference between local and average rates of growth naturally furnished by mechanical stress (Eq. 1). This mode of regulation, which is called “integral feedback” in control theory (47), is the method of choice in engineering design because of its stability properties and insensitivity to parameters (such as details of the pressure dependence of  $\gamma$  as shown in Fig. 3). Stress relaxation due to cell rearrangement and plastic flow ( $\tau^{-1}$  term in Eq. 1), which we have so far neglected in the discussion of the feedback, limits the “memory” of integration making the adaptation of growth rate imperfect. Similar limitation typically applies in the engineering implementation of integral feedback but, provided that relaxation is sufficiently slow, it does not significantly compromise feedback function.

<sup>||</sup>One can imagine an alternative mechanism in which cells communicate their proliferation rate (or their local density) to their neighbors by means of a chemical messenger (or cell contact interaction). However, to compare their own growth rate with that of the surrounding tissue, cells would have to correctly calibrate the received signal by fine tuning signal-transduction parameters.

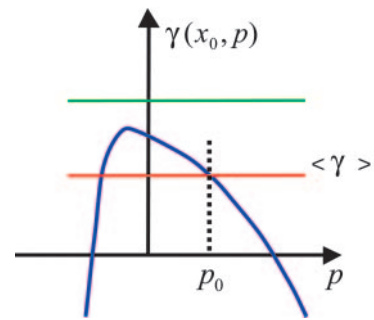


Fig. 3. Pressure dependence of local tissue growth rate (the growth curve) and the feedback effect scenarios. Blue curve represents an assumed growth curve for a mutant clone. Negative  $\gamma$  represents apoptosis. In the case in which background growth rate (red line) is slower than the rate of clone growth, the growth-rate differential leads to the increase of local pressure within the clone until it reaches  $p_0$ , at which the rates of growth for the clone and background equalize. For the case of growth-impaired clones, the rate of background growth (represented by the green line) can be higher than the maximal possible rate of clone growth. The growth-rate differential then leads to a decrease in local pressure and if blue and green curves do not intersect, the rate of growth in the clone cannot catch up with that of the background leading to continuing build-up of negative pressure (i.e., tension). Excessive tension in the tissue and the consequent distortion of cells may trigger apoptosis. This scenario could explain elimination of slow-growing clones by cell competition (6, 11).

### Nonautonomous Effects

We have discussed mechanical feedback on the basis of the quasi-local relation between pressure and the growth rate given by Eq. 1. The latter was derived for idealized 2D elasticity. It is more appropriate to treat epithelial cell layer as an elastic layer of finite thickness. Analysis of in-plane deformations induced by nonuniform growth in this case will modify Eq. 1 by introducing the following term on the left side:  $w^2 \nabla^2 (d/dt)p(r, t)$  with  $w$  being a characteristic length scale comparable with cell size.<sup>\*\*</sup> The effect of this term is to smoothen out any spatial variation of the pressure induced by nonuniform growth, with the characteristic length scale for pressure averaging provided by  $w$  (Fig. 5a).

One consequence of the nonlocality of the induced stress is that if a faster growing mutant clone has generated high level of compression, it will be felt nonautonomously by nearby (i.e., within  $w$  distance from the border) WT cells. If the pressure is sufficiently high, as shown in Fig. 5b, this effect can cause apoptosis in the WT cells surrounding overgrowing clones. Death of surrounding cells would partially relieve the pressure on the clone, allowing additional growth of the mutant clone at the expense of WT tissue. In the case of growth-compromised clones, apoptosis appeared as an inescapable consequence of the inability of the growth compromised cell to catch up with the surrounding tissue (Fig. 3). By contrast, in the present case, the fate of the cells surrounding an overgrowing clone depends on the sensitivity of these cells and those in the overgrowing clone to pressure [i.e., apoptosis is predicted only for the case in which the stabilizing pressure  $p_0$  (see Fig. 5b) exceeds the threshold of apoptosis for the surrounding tissue]. Thus, the mechanical-feedback scenario may provide an explanation for the observed cell-competition phenomena (6, 11, 41, 43) described in the Introduction.

Because mechanical interactions are nonlocal, interaction effects between nonadjacent clones and clones and compartment

<sup>\*\*</sup>This characteristic length does not necessarily correspond to the thickness of the disc, because the elasticity of the tissue is likely to reside in a much thinner apical cytoskeleton layer.



Indeed, cell division occurs randomly throughout the disk tissue (with apparently random orientation of mitotic spindles) (9). The resulting distribution in the number of cells in WT clones of any given age is very broad (48) and must be considered on a logarithmic scale. The latter is to be expected for a multiplicative random process such as cell proliferation. We find that distribution of cell numbers in relatively “young” clones (48) is consistent with division being governed by a two-step Poisson process (i.e., a random process involving two consecutive random steps occurring at the same average rate). As shown in Fig. 4*b*, the variance of the logarithm of the number of cells in a clone behaves differently with and without feedback. In the latter case, variance saturates, whereas in the former case, it would decrease with time after the initial rise.

## Discussion

In the context of mechanical effects, growth-affecting mutations act by means of two parameters, (*i*) rate of cell mass acquisition, or alternatively, the rate,  $\alpha$ , with which cell area would grow (in the absence of mechanical constraint); and (*ii*) average rate of cell division,  $\beta$ . Together, these two parameters determine the average area of a cell,  $\alpha/\beta$ , and the average density of cells,  $n = \beta/\alpha$ . The rate of tissue growth, which featured in tissue growth mechanics discussed above, is given by  $\gamma(r) = \alpha(r)n(r)$  (see *Supporting Appendix* for details), where we explicitly allow for possible positional dependence by means of  $r$ .

Known mutants are often classified as “compensated” (e.g., cyclin D) or “noncompensated” (e.g., PI3K, Myc, RBF, and E2F; ref. 10) depending on whether they coordinate cell growth with division to maintain constant cell size (i.e., constant  $\alpha/\beta$ ). From the point of view of mechanical interactions, we must instead consider effect of mutation on  $\gamma$ . We observe that mutations which affect only cell growth rate  $\alpha$  (without a change in  $\beta$ ) have only a transient effect on  $\gamma$  (within a cell-cycle time of induction) because, in the steady state, the effect of  $\alpha$  on average tissue growth rate would be compensated by the change in local cell density, such that  $\gamma = \alpha n = \beta$ . Only mutations affecting the cell-division rate  $\beta$  affect the tissue-growth rate  $\gamma$  in a steady state. However,  $\alpha$ -type mutants [which, like Myc (10), affect cell size but not rate of cell division] make clones that, while growing at same exponential rate as WT, are still larger (or smaller) than WT by a constant factor. In the absence of any feedback, this factor would be the ratio of mutant to WT single-cell areas. The excess size of such clones would still generate excess local pressure (which, according to Eq. 1, is the integral of growth-rate difference) and reduce the rate of proliferation of cells within and in the vicinity of such clones. If the  $\alpha$ -type mutation causes reduction of cell and clone size, our model predicts that the consequent tensile stress within the clone would reduce its growth rate, causing further increase in tensile stress and eventual elimination of the clone by apoptosis. We expect a major phenotypic difference between mutants to arise from different form of “growth curves”  $\gamma(p)$  for different genotypes. The sensitivity of  $\gamma$  to stress would determine the extent of overgrowth and the extent of apoptosis of surrounding tissue. Dependence of growth rate on stress and resulting cell distortion could account for some of the features of cell competition, as explained above. However, cell competition is likely to be a complex phenomenon, caused not only by the differential growth rate but also by difference in cell identity (11, 43, 49, 50).

The discussion of the mechanical effect of nonuniform growth was based on two fundamental approximations, that (*i*) cells are not free to move within the tissue on the time scale of cell division and (*ii*) the epithelial tissue layer remains flat. If the cells were free to move, all stresses induced by nonuniform growth could be relieved and the mechanism described above would not operate. However, if cell rearrangement (and plastic flow) were slow, all of the above discussion would apply with the sole

modification that mechanical stresses would have a finite “memory” and over-pressure would saturate at a constant value. Here, our discussion was limited to linear elasticity. A more detailed analysis including nonlinear effects can be carried out with the help of numerical simulations. To address the second issue, we note that buckling of a 2D sheet is an instability that requires a finite threshold for local strain. Buckling does not occur in the wing pouch unless normal growth regulation, which preserves tissue planarity, is disrupted. However, reproducible folding in the late stages of normal imaginal disk growth could be naturally attributed to the mechanical effects due to nonuniform growth and spatial modulation of the adhesive properties of the tissue (and, hence, of its mechanical rigidity,  $\mu$ ). It would be interesting to investigate further the role of nonuniform growth in generating 3D tissue structures in animal and plant development (12–14, 51, 52). An interesting extension of the present model would explore the possibility that mechanical feedback effect depends not only on the (2D) pressure but also on the inplane deviatoric stress (46). It is quite possible that the process of cell division is not in itself isotropic; e.g., the direction of mitotic spindle (and the daughter cell axis) may actually be correlated with local in-plane stress axis (15).

It is important to emphasize that the main advantage of mechanical feedback in growth regulation is that it would be driven directly by the nonuniformity of the growth rate. In contrast, any chemical signaling mechanism would require “fine-tuning” (of messenger secretion and signal transduction) for the signal to correctly represent the difference of the growth rate of a cell with that of its neighbors. For example, it has been proposed that cell competition operates through competition for Dpp (53). Although it is true that rapid uptake of Dpp by any cell would have a nonautonomous effect, it would not directly depend on the growth-rate differential but, rather, on the difference of cell identity (e.g., their genetic make up).

Ultimately, one would want to identify the molecular mechanism underlying possible effect of mechanical stress on cell growth and proliferation. An intriguing possibility discussed here focuses on Armadillo ( $\beta$ -catenin), which is known to play central role in the transduction of Wntless (Wnt) signal, which is known to regulate tissue growth and, at the same time, serve as an adaptor in the assembly of the transcellular E-cadherin/actin network (25, 26, 54, 55). Armadillo was implicated also in the transduction of stress effect on expression of Twist in fly embryo (24). Alternatively, transcription factor MalD [and serum response factor (SRF)] (27) has been implicated in mechanical stress-driven response in motile cells and could be a plausible mediator of stress effects in the present context as well. Another recently proposed mechanism of mechanotransduction (56) involves modulation of the growth factor concentration in the intercellular space resulting from compression of the latter by mechanical pressure. Clearly, new experiments are needed to establish the presence of stress induced interaction and its molecular mechanism in growing epithelial tissue.

Last, we note that mechanical feedback on tissue growth, if present, would have a role in the progression of cancer.

## Appendix: Mechanical Stress in Nonuniformly Growing Tissue

On length scales that are large compared with cell size and cell-layer thickness, the deformation of the tissue may be described in a continuum approximation. Let vector  $\Delta u_a(r)$  denote the incremental displacement of a tissue patch (initially at position  $r$ ) after a small time interval  $\Delta t$ . It is determined by minimization of the elastic strain energy given by the following:

$$H = \int d^2r \left\{ \mu \sum_{a,b} \left[ \Delta u_{ab}(r) - \frac{1}{2} \delta_{ab} \Delta u_{cc}(r) \right]^2 + \frac{K}{2} [\Delta u_{cc}(r) - \Delta t \gamma(r)]^2 \right\} \quad [\text{A-1}]$$

where

$$\Delta u_{ab}(r) \equiv \frac{1}{2} \left[ \frac{\partial \Delta u_b(r)}{\partial r_a} + \frac{\partial \Delta u_a(r)}{\partial r_b} \right]$$

is the strain tensor quantifying spatial nonuniformity of  $\Delta u(r)$  (and we are using the convention that repeated indices are summed).  $K$  is the bulk modulus and  $\mu$  is the shear rigidity (47). Tissue displacement is driven by the action of nonuniform tissue growth with a spatially nonuniform rate  $\gamma(r)$  acting over the time interval  $\Delta t$ . This elastic energy minimization is appropriate as long as growth is slow compared with elastic response. Elastic energy,  $H$ , is minimized by displacement vector obeying:

$$\frac{\partial \Delta u_a(r)}{\partial r_a} = \Delta t(1 + \mu/K)^{-1} \gamma(r) + \Delta t \chi(r), \quad [\text{A-2}]$$

with a scalar function  $\chi(r)$  satisfying  $\partial_a^2 \chi = 0$  and determined by the boundary conditions. Eq. A-2 is analogous to electrostatics, with the right side acting like charge density and  $\Delta u_a$  playing the role of electrostatic field. Having determined incremental displacement  $\Delta u_a$ , one can compute the incremental change in pressure:

$$\Delta p = -\Delta t \gamma(r) \frac{\mu K}{K + \mu} + \Delta t \chi(r). \quad [\text{A-3}]$$

Because for uniform growth with free boundary conditions tissue displacement corresponding to uniform dilation  $\Delta u_a(r) = \Delta t \gamma r_a / 2$  accommodates local increase in area without generating any stress we have, for nonuniform growth with free boundaries:

$$\frac{\Delta p(r)}{\Delta t} = -\frac{\mu K}{K + \mu} [\gamma(r) - \langle \gamma \rangle], \quad [\text{A-4}]$$

where  $\langle \gamma \rangle$  is the rate of growth averaged over the tissue. The first term explicitly shows that local pressure is driven by the difference between local growth rate and the average growth rate and that it arises through the action of shear rigidity  $\mu$ . A more detailed derivation and discussion is given in *Supporting Appendix*.

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